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Chapter 5

Aquaporin Biomimetic Membranes

Amira Abdelrasoul, Huu Doan and Ali Lohi

Abstract

Recent research looked at an array of aquaporin protein structures, their unique functions, and potential applications in the research and industrial sectors. This chapter focuses on the specific functional features of aquaporin biomimetic membranes to interrogate their permeability properties in relation to various biomimetic water-transporting membranes. This chapter discusses in detail functional characteristics of aquaporin, how to produce it, and the status of aquaporin development.

Keywords: aquaporin, function, permeability, protein, membrane design

1. Introduction

A series of recent reviews looked at an array of aquaporin protein structures, their unique functions, and potential applications in the research and industrial sectors [1–5]. This chapter focuses on the specific functional features of aquaporin biomimetic membranes to interrogate their permeability properties in relation to various biomimetic water-transporting membranes.

Aquaporin protein structures are a family of 24–30 kDa pores that form an essential type of membrane proteins. The process of red blood cell membrane protein purification (channel-forming key membrane protein of 28 kDa or CHIP28) [6] and consequent form of this protein in Xenopus oocytes [7] and liposomes [8] showcased a rather quick water diffusion process along the osmotic gradients. Since this process of purification, new research data had become available on this specific class of proteins, and a term aquaporins came to define it [9]. The primary aquaporin sequence features two repetitions where each one includes three transmembrane spanning α-helices (TM 1–3), as shown in Figure 1. Every repetition section includes a loop between TM2 and TM3 and an asparagine-proline-alanine (NPA) pattern signature.
The aquaporin protein is assembled in a form of a hour-glass-shaped structure with six TM segments encircling a pore structure in the center and demarcated by the two opposing NPA motifs, as reflected in Figure 1a and b. The conserved aromatic/arginine (ar/R) region effectually describes the selectivity filter or constriction site, which is channel lumen’s the narrowest part. The six TM AQP unit becomes a functional entity that acts as a pore, with the predominate unit assembly in biological membranes as a tetrameric arrangement [10], as indicated in Figure 1c and d. Due to their specific permeability properties, the mammalian homologs are categorized into two factions of aquaglyceroporins and aquaporins. The Escherichia coli model system can include both of these variants [11], the orthodox ‘water only’ channel AqpZ [12, 13], and the aquaglyceroporin GlpF, which is likewise permeable to glycerol [14]. While certain aquaporins may be categorized as solely water channels (e.g., AQP0, AQP4, and AqpZ), research that is being currently conducted indicates that a high number of aquaporins can have supplementary permeability properties [4].

Figure 1. Aquaporin protein structure. (a): Side view of AqpZ monomer. Protein backbone (deep teal) with the two terminal asparagines from the NPA motifs shown using stick representation and the ar/R selectivity filter residues displayed in space fill representation. For stick and space fill representations, atoms have been color-coded as follows: carbon (green), oxygen (red), and nitrogen (blue). (b): Top view illustrating the selectivity filter (or constriction site) created by the four amino acids: F43, H174, R189, and T183. (c–d): Side and top view of the tetrameric AqpZ complex with the four monomers depicted in deep teal, violet purple, pale green, and yellow [1].
Supplementing their already complex permeability profile parameters, multiple aquaporins showed a number of gating forms comparable to the opening and closing dynamics occurring in ion channels induced by external stimuli [15]. While numerous aspects of aquaporin gating and the process of regulating their permeability capacity remain unknown, the overall functionality of certain aquaporins has been confirmed as contingent on calmodulin [16, 17], phosphorylation, [18, 19] and pH [16, 20, 21].

2. Functional characterization of aquaporins

The properties of water’s permeability and solute’s rejection of single aquaporins cannot be measured very easily. Molecular dynamic simulations conducted with aquaporins suggest diffusional water permeabilities that correspond to the transport of $10^8$–$10^9$ water molecules/s [22]. With regard to the quantity of the transported molecules, this data is about an order of magnitude greater than the parameters available in standard ion channel, with a single channel at a picoampere (pA) current level and a millisecond (ms) time scale corresponding to the transmembrane displacement of $10^7$ ions [23]. Although currents in the pA range can be calculated using the standard patch-clamp methods, the movement of $10^8$–$10^9$ water molecules is not experimentally available due to the limitations of methods presently available to researchers. On the other hand, the macroscopic transport mediated with the aid of an ensemble of aquaporins can be measured. After this assessment is applied, the measured osmotic transport arising from a large (known) number of aquaporins can help estimate the single aquaporin permeability values. The two methods currently implemented for these calculations are as follows: Xenopus oocyte volume change, and light scattering from the proteoliposomes/proteopolymersomes.

In the Xenopus oocyte method expression, frog oocytes (~1 mm diameter) are cytoplasmically injected with mRNA that has been transcribed in vitro from a cDNA clone [24]. For aquaporins, in this instance, the resultant expression makes the oocyte membrane substantially more water permeable in comparison to the control oocytes [7]. During an osmotic challenge, the oocyte will alter its size (diameter value) and by implementing small osmotic gradients for brief period of time (e.g., 2.5 number of milliosmoles (mosM) for 5 s), the transport parameters (solute rejection and water permeability) can be calculated based on the initial rate of oocyte volume change rates in terms of shrinkage and swelling experimental runs [25].

Water permeability values of proteoliposomes/proteopolymersomes could likewise be assessed through the process of identifying the light scattering of the preparations within a stopped-flow apparatus setup, as indicated in Figure 2a. A suspension of aquaporin-containing vesicles of an original diameter approximately 200 nm briskly mixed with an identical volume of hyperosmolar solution featuring membrane impermeable solutes (e.g., sorbitol, sucrose, or mannitol) for proteoliposomes can create a dynamic where the subsequent transmembrane osmotic gradient will create water efflux from vesicles. As a result, the vesicle volume is lowered and may be measured with the help of an increase in the intensity values of scattered light. The rate constant, $k$, of the surge in normalized light intensity values is symptomatic of the water permeability coefficient and the water efflux rate constant. In this
instance, the light intensity values increase in an exponential manner with time, as indicated in Figure 2b. The response from the protein-free controls is connected to a single exponential, while the double-exponential function is applied for proteoliposomes/proteopolymersomes (vesicles) reflecting the dual pathways for water transport, either protein mediated or membrane mediated. Based on these processes, the k values can then be implemented for the calculation of the osmotic permeability $P_f$:

$$P_f = \frac{k}{S/V_0, V_w, \Delta \text{osm}}$$

where $S/V_0$ is the surface area of the initial volume ratio of the vesicle, $V_w$ is the partial molar volume of water (18 cm$^3$/mol), and $\Delta \text{osm}$ is the variance in osmolarity between the intravesicular and extravesicular aqueous solutions. Based on stopped-flow measurements, the water permeability of AqpZ is predicted to be in the range of 2–10 × 10$^{-14}$ cm$^3$/s [27–29] and showed a reasonable agreement with previously reported molecular dynamics simulation results (3–30 × 10$^{-14}$ cm$^3$/s).

3. Production of aquaporins

Currently, the majority of recombinant aquaporins have only been created in lab-scale quantities for the purposes of screening, regulatory, functional, or structural research studies [30, 31]. The primary concern in protein production is that the membrane protein overexpression in vivo is problematized by their overly complex structure, hydrophobic transmembrane regions with host toxicity, and the low efficiency and time-consuming refolding steps necessary. Advances in high-expression systems and their potential applications could offer an insight into how a large-scale AQP production and implementation could be facilitated. These high-expression systems include E. coli, Pichia pastoris, Saccharomyces cerevisiae, and baculovirus/insect cell-based systems, and their recent review is available for additional information [32].
The E. coli expression-based methodologies that produce milligram quantities of protein have been effectively used to analyze the X-ray structure of the AqpZ and GlpF channels, AqpZ [13], GlpF [14], and of the archaeal aquaporin AqpM [33]. A high level of expression (200 mg/L) of the traditional aquaporin AqpZ was achieved in a recent study of the E. coli system, where a maltose binding protein (MBP) was used as a fusion partner protein, followed by a condition optimization process [34]. The S. cerevisiae system can be utilized for the production of large amounts of functional aquaporins [30, 35–39]. Alternatively, the methylotrophic yeast P. pastoris has been effectively used to produce a high number of distinct aquaporins. The potentially produced selection includes all 13 human aquaporins [40] and a wide range of active plant aquaporins [41–47]. Large-scale expressions of various functional recombinant aquaporins have been obtained with the aid of a baculovirus/insect cell system [48–55].

Research data indicate that there is a possibility for high-level membrane protein expression based on cell-free (CF) type of production. The essential requirement in this case is the process of synthesizing membrane proteins together with natural or synthetic lipids, as well as detergents, that can help solubilize the membrane’s protein content. CF type of aquaporin production has been illustrated at analytical levels [31, 56–58], and recent tests showed high expression of properly folded AqpZ. Furthermore, plant aquaporin has been achieved with E. coli CF protocols and implementing various fusion vectors [59, 60]. Milligram of high potential AqpZ have been created in synthetic liposomes by using a CF approach [61]. Sutro Biopharma Inc. [62] showed the possibility of cost-effective cell-free protein synthesis in a 100-l reaction and the implicit advantages offered by CF systems that can act as an effective recombinant protein in industrial-scale production platforms.

The protein, that has been stabilized using a detergent, must be modified into its host biomimetic membrane; however, this creates challenges for industrial scaling and production. These challenges may be defined in terms of the detergent-stabilized intermediates, where the detergent cost and stability become primary concerns [63, 70]. Alternatively, the process of optimizing the interaction between membrane, protein (c.f. [64–66]), and yield may directly affect how much of functional protein content can be integrated into the final product (c.f. [67]).

4. Status of the aquaporin membrane development

Research conducted by Tang et al. suggests that membranes with excessively high salt rejection and permeability values can be created with the aid of aquaporin protein [68]. The measured water permeability values of AqpZ with proteoliposomes are used by researchers to argue that AqpZ-based biomimetic membranes can, in theory, obtain a membrane permeability as high as 167 μm·s⁻¹·bar⁻¹ (i.e., 601 L·m⁻²·h⁻¹·bar⁻¹, as shown in Figure 3). This value is more permeable by about two orders of magnitude when compared to the preexisting commercially available seawater RO membranes [69]. Even though there is a high level of membrane permeability present, there are considerable scaled-up concerns remaining. This is primarily due to the fact that the membranes are built using nanoscale elements, that is, aquaporins, and there are serious questions about how the biomimetic membranes can be scaled up and then stabilized to about 1 m² dimensions appropriate for industrial applications.
Multiple design methods have been planned for the foreseeable future, as outlined in Figure 4. These strategies incorporate the creation of membranes based across multiple micron scale apertures, possibly as freestanding lipid or polymer membranes [44, 53, 68, 69], or alternatively as membranes stabilized using polymeric support materials [70]. Additional methods depend on nanoporous support materials on top of which the membranes are placed. For example, in this approach, there are several variations. The charged lipid vesicle can be deposited onto the commercially available nanofiltration membranes where the recipient surface is either a crosslinked polyamide or a sulfonated polysulfone negatively charged at pH7 [71]; there is an active rupture of aquaporin-containing polymersomes on top of the methacrylate functionalized cellulose acetate membranes [72], the method where detergent-stabilized tagged aquaporin are introduced into monolayers with nickel-chelating lipids [73]; and proteopolymersome deposition onto the surface of polycarbonate track-etched substrates covered with gold and then functionalized using photoactive acrylate groups. Research data suggest that [71–73] the implementation of spin coating and applied pressure improves vesicular coating/fusion on the substrate. As part of this process, surface charge and hydrophilicity values have been proven to play an essential role in shaping the overall quality of the supported lipid layers.

The data outlined in Table 1 show the existing methods of creating aquaporin-based biomimetic membranes. In the majority of cases, most of the membranes discussed earlier feature a relatively low NaCl rejection value (or the rejection information is not available), a dynamic that prevents them from being used in desalination processes. Moreover, a large number of these membranes are not sufficiently stable for sophisticated industrial applications. In most cases, only small membrane areas are prepared, and the majority of methods depend on the implementation of specialized nanofabrication approaches, making the process exceedingly complicated and excessively expensive for scale up in forward osmosis (FO) and RO membrane fabrication. Ongoing innovation has allowed for the development of a new approach in the process of fabricating aquaporin-based biomimetic membranes. This innovative method relies on embedding aquaporin-containing proteopolymersomes or proteoliposomes into a

Figure 3. Comparison of water permeability of polymer vesicles with AqpZ (AqpZ-ABA) and without AqpZ (ABA) to those present in polymeric membranes [69].
crosslinked polyamide matrix \[69, 71\]. In this approach, a microporous substrate was first soaked in an aqueous solution of m-phenylene-diamine (MPD) that likewise includes some aquaporin-containing vesicles, as shown in Figure 4. These soaked substrates were subsequently exposed to a tri-mesoyl chloride (TMC) solution to allow the formation of an interfacially polymerized polyamide rejection layer with vesicles dispersed in a thin rejection layer.

As part of this design, the aquaporin-containing vesicles offer superior water pathways through the polyamide layer and as a result substantially improve the membrane’s water capacity for permeability. Furthermore, the crosslinked polyamide provides a scaffold that maintains the

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**Figure 4.** Summary of the existing biomimetic membrane designs. (a): Cross-sectional examples of solid-supported biomimetic membranes. (i) Direct deposition on a hydrophilic surface (light gray). This technique may introduce part of the integral membrane proteins (red protein shaded areas) embedded in the matrix formed from the self-assembly of lipids (dark gray molecules) too close to the surface, potentially inactivating (or even denaturing) the protein. (ii) Cushion-supported biomimetic membrane. (iii) Layers grafted covalently onto the support using spacers with silane groups and reacting with hydroxyl surfaces (light gray), or spacers with thiol groups bonding on gold surfaces (orange). Various hydrophilic spacers (e.g., poly(ethylene glycol) (PEG)) may be applied as cushion material. This cushion can be noncovalently interacting with the biomimetic membrane (yellow spacers) or covalently attached to lipids (red lipid headgroups) or proteins (green bonds), in the biomimetic membrane directly or through intermediates, for example, biotin-avidin complexes. (b): Cross-sectional illustrations of porous supported biomimetic membranes with an embedded protein (blue). (i) Freestanding membrane formed across a (micro or nano) porous support section. The membrane (solvent-free or solvent-containing) is formed in an aperture (light gray). (ii) Hydrogel-encapsulated biomimetic membrane. A hydrogel polymer meshwork (yellow) encapsulating the biomimetic membrane. (iii) A surface (S) layer-encapsulated membrane. The monomolecular layer of protein or glycoproteins (red) self-assembles into a two-dimensional lattice creating identical pores 2–8 nm in diameter. (iv) A cushioned membrane on a porous support \[70, 71\].
<table>
<thead>
<tr>
<th>Approach</th>
<th>WP (L·m⁻²·h⁻¹·bar⁻¹)</th>
<th>RNaCl (%)</th>
<th>Area (cm²)</th>
<th>P_max (bar)</th>
<th>Upscaling issues</th>
<th>Remarks</th>
<th>Ref.</th>
</tr>
</thead>
<tbody>
<tr>
<td>Charged lipid mixture vesicles depositions onto NF membranes</td>
<td>0.83</td>
<td>n.d.</td>
<td>3.5</td>
<td>10</td>
<td>Difficult to produce large defect-free membranes</td>
<td>No aquaporin incorporated</td>
<td>[11]</td>
</tr>
<tr>
<td>Vesicle fusion facilitated by hydraulic pressure on hydrophilic NF membranes coated with positively charged lipids</td>
<td>3.6 ± 0.2</td>
<td>35 ± 8</td>
<td>12.6</td>
<td>1</td>
<td>Difficult to produce large defect-free membranes</td>
<td>Low R_{NaCl} Only suitable for NF, WP/RNaCl not tested. Not suitable for RO.</td>
<td>[67]</td>
</tr>
<tr>
<td>Membranes across multiple micron scale apertures either as free-standing lipid or polymer membranes</td>
<td>n.d.</td>
<td>n.d.</td>
<td>4</td>
<td>n.d.</td>
<td>Nanofabrication required Low robustness</td>
<td>WP/RNaCl not tested. Not suitable for RO.</td>
<td>[66, 67]</td>
</tr>
<tr>
<td>Membranes across multiple micron scale apertures and stabilized by hydrogel encapsulation</td>
<td>12-40</td>
<td>n.d.</td>
<td>3.5</td>
<td>2</td>
<td>Nanofabrication required. High robustness</td>
<td>Characterized with gramicidin channels. No aquaporin incorporated.</td>
<td>[18]</td>
</tr>
<tr>
<td>Aquaporin containing polymersomes on methacrylate functionalized CA membranes</td>
<td>34.2 ± 6.9</td>
<td>32.9 ± 9.1</td>
<td>0.07</td>
<td>5</td>
<td>Medium robustness</td>
<td>Small area. High WP but low R_{NaCl} Only suitable for NF.</td>
<td>[17]</td>
</tr>
<tr>
<td>Detergent-stabilized His-tagged aquaporin added to monolayers with nickel-chelating lipids</td>
<td>n.d.</td>
<td>n.d.</td>
<td>n.d.</td>
<td>n.d.</td>
<td>Complex fabrication. Low robustness</td>
<td>WP/RNaCl not tested. May not be suitable for desalination.</td>
<td>[31]</td>
</tr>
<tr>
<td>Proteopolysomc deposition onto gold-functionalized PC track-etched substrates</td>
<td>n.d.¹</td>
<td>n.d.²</td>
<td>0.096</td>
<td>n.d.</td>
<td>Complex fabrication. Low robustness</td>
<td>Small area. Relatively high WP in FO. No RO data.</td>
<td>[35]</td>
</tr>
<tr>
<td>Interfacial polymerization method with embedded proteoliposomes</td>
<td>4 ± 0.4</td>
<td>96.3 ± 1.2</td>
<td>&gt;200</td>
<td>14</td>
<td>Simple fabrication. High robustness</td>
<td>Combined high WP and RNaCl. Suitable for RO.</td>
<td>[8]</td>
</tr>
</tbody>
</table>

¹Including membrane scaffold.
²RO tests were not performed. Based on FO tests, a WP of 16.4 L·m⁻²·h⁻¹ and a salt flux of 6.6 g·m⁻²·h⁻¹ were obtained for membranes prepared with a protein-to-polymer molar ratio of 1:100, with 0.3 M sucrose as draw and 200 ppm NaCl as feed.

Table 1. Existing approaches for the preparation of aquaporin-based biomimetic membranes. Performance data are presented as water permeability (WP) [L·m⁻²·h⁻¹·bar⁻¹], NaCl rejection (RNaCl) [%], membrane area (A) [cm²], and maximal external pressure applied (PMax) [bar] when operated in RO. CA: cellulose acetate, PC: polycarbonate.
aquaporin-containing vesicles as well as defends them against the surrounding environmental conditions. This dynamic is anticipated to considerably increase the membrane’s overall stability. This type of membrane exhibited a permeability value of ~4 L∙m⁻²∙h⁻¹∙bar⁻¹, as shown in Table 1, while maintaining similar or even superior NaCl rejection values. This permeability is ~40% greater than the one occurring in commercial brackish water reverse osmosis membrane BW30 that was tested in the same conditions. Membranes featuring such a design have been extensively tested and showed enhanced stable flux and rejection performance capacity for the specified durations of weeks and months. A noticeable water improvement effect of aquaporins was likewise confirmed through a comparative analysis with membranes featuring vesicles containing inactive R189A AqpZ mutants [69–71]. This straightforward quality of this fabrication procedure ensures that this technique can be effortlessly scaled up for the manufacturing of large membrane areas crucial for industrial applications.

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